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	CR TO THE UNITED STATES	1141/61930
DESIGNATED/ELECTED OFFICE (DO/EO/US)		U.S. APPLICATION NO. (If known, see 37 CFR 1.5)
CONCERNING A FILING UNDER 35 U.S.C. 371		1 09/554155
INTERNATIONAL APPLICATION NO.	INTERNATIONAL FILING DATE	PRIORITY DATE CLAIMED
PCT/JP98/05406	12/01/98	12/01/97
TITLE OF INVENTION  MAGNET APPARATUS AND MRI A	APPARATUS	
APPLICANT(S) FOR DO/EO/US		
1) Hitachi Medical Corpor		lawing items and other information.
· · ·	tes Designated/Elected Office (DO/EO/US) the foll ans concerning a filing under 35 U.S.C. 371.	owing terms and other information:
	ENT submission of items concerning a filing under	r 35 U.S.C. 371.
This express request to begin nation	nal examination procedures (35 U.S.C. 371(f)) at a	my time rather than delay
examination until the expiration of A proper Demand for International	the applicable time limit set in 35 U.S.C. 371(b) a Preliminary Examination was made by the 19th m	and PCT Articles 22 and 39(1).
	lication as filed (35 U.S.C. 371(c)(2))	
a. X is transmitted herewith (required only if not transmitted by the International Bureau). b. As been transmitted by the International Bureau.		
b. has been transmitted by the international Bureau.  c. is not required, as the application was filed in the United States Receiving Office (RO/US).		
6. A translation of the International Application into English (35 U.S.C. 371(c)(2)).		
7. Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371(c)(3))		
a. are transmitted herewith have been transmitted by a have not been made; how	(required only if not transmitted by the Inter	rnational Bureau).
b. have been transmitted by	y the International Bureau.	
c X have not been made; however, the time limit for making such amendments has NOT expired.		
d. have not been made and will not be made.		
A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).		
9. X An oath or declaration of the inve		
A translation of the annexes to the (35 U.S.C. 371(c)(5)).	e International Preliminary Examination Rep	port under PCT Article 36
Items 11. to 16. below concern document		
1. 🛣 An Information Disclosure Statem	ent under 37 CFR 1.97 and 1.98.	
2. X An assignment document for recor	rding. A separate cover sheet in compliance	with 37 CFR 3.28 and 3.31 is included.
3. A FIRST preliminary amendment.		
A SECOND or SUBSEQUENT pro	eliminary amendment.	
4. A substitute specification.	•	
5. A change of power of attorney and	or address letter.	
12/01/98; copy of Internation	ress Mail Certificate; copy of onal Search Report; English tr 1998) and cited references; Eng	anslation of Search

# PTO/PCT Rec'd 2 2 AUG 2000

Dkt. 1141/61930

#### IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Application of:

KAKUGAWA, et al.

Serial No.

09/554,155

Group Art Unit:

Date Filed

May 9, 2000

Examiner:

For

MAGNET APPARATUS AND MRI APPARATUS

1185 Avenue of the Americas New York, N.Y. 10036

Assistant Commissioner for Patents

**Box PCT** 

Washington, D.C. 20231

### PRELIMINARY AMENDMENT

Sir:

Please amend the application as follows:

### In the Claims:

Please add new claims 22-65 as follows:

--22. (New) A magnet device according to claim 4, characterized in that each of the static magnetic field generation sources includes at least one ferromagnetic body which helps formation of the magnetic field.--

I hereby certify that this paper is being deposited this date with the U.S. Postal Service as first class mail addressed to the Assistant Commissioner for Patents, Washington, D.C. 20231.

Ivan S. Kavrukov

Ivan S. Kavrukov Reg. No. 25,161 Date

--23. (New) A magnet device according to claim 5, characterized in that each of the static magnetic field generation sources includes at least one ferromagnetic body which helps formation of the magnetic field.--

- --24. (New) A magnet device according to claim 6, characterized in that each of the static magnetic field generation sources includes at least one ferromagnetic body which helps formation of the magnetic field.--
- --25. (New) A magnetic device according to claim 19, characterized in that the ferromagnetic body functions as a magnetic pole.--
- --26. (New) A magnetic device according to claim 20, characterized in that the ferromagnetic body functions as a magnetic pole.--
- --27. (New) A magnetic device according to claim 21, characterized in that the ferromagnetic body functions as a magnetic pole.--
- --28. (New) A magnetic device according to claim 22, characterized in that the ferromagnetic body functions as a magnetic pole.--

- --29. (New) A magnetic device according to claim 23, characterized in that the ferromagnetic body functions as a magnetic pole.--
- --30. (New) A magnetic device according to claim 24, characterized in that the ferromagnetic body functions as a magnetic pole.--
- --31. (New) A magnet device according to claim 1, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--
- --32. (New) A magnet device according to claim 2, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--
- --33. (New) A magnet device according to claim 3, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--

Page 4

--34. (New) A magnet device according to claim 4, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--

- --35. (New) A magnet device according to claim 5, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--
- --36. (New) A magnet device according to claim 6, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.--
- --37. (New) A magnet device according to claim 31, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.--
- --38. (New) A magnet device according to claim 32, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped

ferromagnetic body.--

- --39. (New) A magnet device according to claim 33, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.--
- --40. (New) A magnet device according to claim 34, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.--
- --41. (New) A magnet device according to claim 35, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.--
- --42. (New) A magnet device according to claim 36, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.--
- --43. (New) A magnet device according to claim 1, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying

means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--

- --44. (New) A magnet device according to claim 2, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--
- --45. (New) A magnet device according to claim 3, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--
- --46. (New) A magnet device according to claim 4, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--

- --47. (New) A magnet device according to claim 5, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--
- --48. (New) A magnet device according to claim 6, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.--
- --49. (New) An MCI device which uses the magnet device according to claim 1.--
- --50. (New) An MCI device which uses the magnet device according to claim 2.--
- --51. (New) An MCI device which uses the magnet device according to claim 3.--
- --52. (New) An MCI device which uses the magnet device according to claim 4.--
- --53. (New) An MCI device which uses the magnet device according to claim 5.--

- --54. (New) An MCI device which uses the magnet device according to claim 6.--
- --55. (New) An MCI device including the magnet device according to claim 1, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.--
- --56. (New) An MCI device including the magnet device according to claim 2, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.--
- --57. (New) An MCI device including the magnet device according to claim 3, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of the stand on which a measurement object is laid.--
- --58. (New) An MCI device including the magnet device according to claim 4, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.--
- --59. (New) An MCI device including the magnet device according to claim 5, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.--

- --60. (New) An MCI device including the magnet device according to claim 6, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.--
- --61. (New) A super conducting magnetic device for an open and vertical magnetic field type MCI device including a first and a second static magnetic field generation source which are disposed in vertical direction opposing each other while sandwiching a space for receiving a person to be inspected, each of the first and second static magnetic field generation sources includes static magnetic field generation use coil units of equal to or more than three which are arranged concentrically around the center axis in vertical direction thereof, characterized in that, the directions of DC current flow in the static magnetic field generation use coil units of equal to or more than three in each of the static magnetic field generation sources are determined alternative in positive and negative direction with reference to projection positions of geometric centers of cross sections of the respective coil units of equal to or more than three on a straight line passing through a crossing point, on a plane which is perpendicular to the center axis in vertical direction and contains a horizontal axis having an equal distance both from the first and second static magnetic field generation sources, of the center axis and the horizontal axis and at the side of the straight line away from the horizontal axis when viewed from the respective coil units of equal to or more than three.—
- --62. (New) A super conducting magnet device for an open and vertical magnetic field type MCI device including a pair of static magnetic field generation sources which are disposed in vertical

direction opposing each other while sandwiching a space having a broad opening for receiving a person to be inspected, and each of the pair of static magnetic field generation sources includes a main coil unit for the static magnetic field generation having a first diameter and being disposed concentrically with the center axis in vertical direction thereof, a plurality of coil units for irregular magnetic field correction each having a diameter smaller than the first diameter and being likely disposed concentrically with the center axis in vertical direction thereof and a shielding coil unit for suppressing magnetic field leakage having substantially the same diameter as the first diameter and being disposed concentrically with the center axis in vertical direction thereof but being located distant position than the main coil unit for static magnetic field generation with respect to the space, characterized in that, the directions of DC current flow in the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic field correction in each of the static magnetic field generation sources are determined alternative in positive and negative direction with reference to projection positions of geometric centers of cross sections of the main coil unit for static magnetic field generation and the plurality of the coil units for irregular magnetic field correction on a straight line passing through a crossing point, on a plane which is perpendicular to the center axis in vertical direction and contains a horizontal axis having an equal distance both from the first and second static magnetic field generation sources, of the center axis and the horizontal axis and at the side of the straight line away from the horizontal axis when viewed from the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic field correction, as well as the direction of DC current flow in the shielding coil unit is determined to be opposite to the direction of the DC current flow in the main coil unit for static magnetic field

generation .--

--63. (New) A magnetic device including a pair of static magnetic field generation sources for

generating a uniform magnetic field directing in a first direction in a finite region each of the static

magnetic field generation sources being provided with at least two current carrying means disposed

concentrically, characterized in that, the at least two current carrying means are disposed

concentrically while being spaced each other and further when assuming a crossing point of a first

axis which is in parallel with the first direction and passes substantially the center of the current

carrying means and a second axis which crosses the first axis orthogonally and locates at

substantially the equal distance from the respective static magnetic field generation sources as a first

point, the current carrying means are disposed in such a manner that when geometrical centers of

cross sections of the current carrying means are projected on a first straight line on a first plane

containing the first axis, the second axis and the first point and passing through the first point, the

current carrying means at the respective corresponding projections aligns alternatively in positive

and negative direction on the first straight line.--

--64. (New) A super conducting magnetic device for an open and vertical magnetic field type

MCI device including a first and a second static magnetic field generation source which are disposed

opposing each other while sandwiching a space for receiving a person to be examined, each of the

first and second static magnetic center axis passing through the center thereof, characterized in that,

the static magnetic field generation use coil units of equal to or more than three in each of the static

magnetic field generation sources are arranged in such a manner that within an angle range defined by a first line segment on a plane containing the center axis and extending in a direction perpendicular to the center axis from a center point on the center axis having substantially the same distance from both first and second static magnetic field generation sources and a second line segment extending from the center point toward the static magnetic field generation use coil unit located most inside and most close with respect to the space within the plane, when the geometric centers of the cross sections of the respective static magnetic field generation use coil units are projected on any straight line while locating the first line segment therebetween, the current flow directions of the static magnetic field generation use coil units at the respective corresponding projection points align alternatively in positive and negative direction on the straight line.—

--65. (New) A super conducting magnet device for an open and vertical magnetic field type MCI device including a pair of static magnetic field generation sources which are disposed opposing each other while sandwiching a space having a broad opening for receiving a person to be examined, and each of the pair of static magnetic field generation sources includes a main coil unit for the static magnetic field generation having a first diameter and being disposed concentrically with the center axis passing the center of the static magnetic field generation sources, a plurality of coil units for irregular magnetic field correction each having a diameter smaller than the first diameter and being disposed concentrically with the center axis thereof and a shielding coil unit for suppressing magnetic field leakage having substantially the same diameter as the first diameter and being disposed concentrically with the center axis thereof but being located distant position than the main

coil unit for static magnetic field generation with respect to the space, characterized in that, the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic field correction in each of the static magnetic field generation sources are arranged in such a manner that within an angle range defined by a first line segment on a plane containing the center axis and extending in a direction perpendicular to the center axis from a center point on the center axis having substantially the same distance from both first and second static magnetic field generation sources and a second line segment extending from the center point toward the coil unit for irregular magnetic field correction located most inside and most close with respect to the space within the plane, when the geometric centers of the cross sections of the main coil unit for static magnetic field generation and the plurality of unit coils for irregular magnetic field correction are projected on any straight line while locating the first line segment therebetween, the current flow directions of the main coil unit for static magnetic field generation and the plurality of unit coils for irregular magnetic field correction at the respective corresponding projection points align alternatively in positive and negative direction on the straight line as well as the direction of DC current flow in the shielding coil

### **REMARKS**

unit is determined to be opposite to the direction of the DC current flow in the main coil unit for

Claims 1-65 are pending in this application.

static magnetic field generation .--

The Office is hereby authorized to charge any fees that may be required in connection with this preliminary amendment and to credit any overpayment to our Deposit Account No. 03-3125.

If a petition for an extension of time is required to make this response timely, this paper should be considered to be such a petition, and the Commissioner is authorized to charge the requisite fees to our Deposit Account No. 03-3125.

If a telephone interview could advance the prosecution of this application, the Examiner is respectfully requested to call the undersigned attorney.

Entry of this preliminary amendment and allowance of this application are respectfully requested.

Respectfully submitted,

Ivan S. Kavrukov Reg. No. 25,161

Attorney for Applicants Cooper & Dunham LLP

Tel.: (212) 278-0400

## 416 Rec'd PCT/PTO 0 9 MAY 2000

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# TITLE OF THE INVENTION Magnet Apparatus and MRI Apparatus

### FIELD OF THE INVENTION

The present invention relates to a super conducting magnet which is suitable for a nuclear magnetic resonance imaging (hereinafter, simply called as MRI) device, and, more specifically, relates to a super conducting magnet device which is provided with a broad opening as well as makes easy to access to a measurement object by reducing the outer diameter of the magnet.

### BACKGROUND ART

15 Conventionally, it was difficult that a person performing inspection such as a medical accesses a person under inspection during image taking with MRI device, therefore, an the so called Interventional Radiology (hereinafter, simply called 20 as IVR) was as well as difficult.

For example, JP-A-7-106153 (1995) entitled "C Type Super Conducting Magnet" discloses a conventional art for avoiding the above problems.

The above referred to device takes MRI images 25 after inserting a patient between two magnetic poles.

This device is for generating a uniform magnetic field by optimizing the configuration of the magnetic

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poles, however, because of weight limitation thereof, a uniform magnetic field space which can be used merely for inspecting a head portion of the patient is generally created.

However, in a case of whole-body use MRI device which permits an image taking of such as the abdomen, bi-shoulder of chest and the patient the a representing an inspection object without moving the patient during image taking, it is generally necessary 10 to generate a uniform magnetic field with intensity variation of a few ppm (for example 2~3 ppm) in an image taking region covered by a sphere having a diameter from 40cm to more than 50cm. Accordingly, it is required to develop an MRI device having a magnet 15 which can generates a uniform magnetic field with its intensity variation of a few ppm (for example, 2~3 ppm) in an image taking region covered by a sphere having a diameter from 40cm to more than 50cm while keeping a highly open space feeling in the magnet for an MRI device.

As has been explained above, it was difficult until now to generate a uniform magnetic field over a broad region in a magnet having a broad opening which an open space feeling for a person to be gives (a patient) representing a measurement inspected (image taking) object. Further, there is a problem to have to increase the outer diameter of the magnet in order to obtain a broad uniform magnetic field space, which causes other problems to deteriorate the open space feeling for the patient and easy access thereto. Still further, when it is intended to enlarge the uniform magnetic field region, which causes a problem of increasing the manufacturing cost of the magnet because the absolute value of magnetomotive forces of coils constituting the magnet has to be increased.

Further, JP-A-3-141619 (1991) discloses a magnet for generating a uniform magnetic field in a broad region in which currents in opposite directions are flown through two coils disposed in outside and inside along a same axis to generate magnetic fields in opposite direction and to superposed the same each other, thereby, a non-uniformity of magnetic field produced by a single coil is canceled out to enlarge a uniform magnetic field region.

Further, JP-A-9-153408 (1997) applied by the present applicants discloses a super conducting magnet 20 device each of a pair of static magnetic field generation sources disposed in vertical direction so as to oppose each other is constituted so as to include one main coil unit for generating static magnetic field and a plurality of coil units for correcting irregular magnetic field, however, JP-A-9-153408 (1997) does not disclose specifically the DC current flow direction in these two sorts of unit

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coils.

### SUMMARY OF THE INVENTION

An object of the present invention is to provide a super conducting magnet with a broad opening used unclear magnetic resonance which generates desirable uniform magnetic field in comparison with a conventional magnet and shows a high open feeling through a small outer diameter of the magnet.

A first aspect of the magnet device according to the present invention which achieves the above object in which two static magnetic sets of generation sources, each being constituted by current carrying means disposed substantially concentrically 15 with respect to a first direction in order to generate uniform magnetic field directing in the direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field 20 generation sources is provided with at least four current carrying means, is characterized in that when assuming a crossing point of a first axis which is in and parallel with the first direction substantially the center of the current carrying means second axis which crosses the first axis and а orthogonally and locates at substantially the equal distance from the two sets of the static magnetic

field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a when geometrical manner that, centers of sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying 10 means corresponding to the respective projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction.

A second aspect of the magnet device according to the present invention in which two sets of static magnetic field generation sources, each being constituted by current carrying means and shielding current carrying means for suppressing leakage magnetic field to an external region disposed 20 substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and 25 each of the static magnetic field generation sources is provided with at least four current carrying means and at least one shielding current carrying means, is

characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses orthogonally and locates axis 5 the first substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, second axis and the first point and passing the through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the 15 current carrying means corresponding to the respective projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction.

A third aspect of the magnet device according to 20 the present invention in which two sets of static each being field generation sources, magnetic means carrying constituted current by substantially concentrically with respect to a first 25 direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing

the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with a ferromagnetic body functioning as a magnetic pole and at least two current carrying means, is characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at 10 substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, second axis and the first point and passing the through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the 20 current carrying means corresponding to the respective projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction.

A fourth aspect of the magnet device according to the present invention in which two sets of static 25 sources, each generation magnetic field constituted by current carrying means and shielding

current carrying means for suppressing leakage field to magnetic an external region disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with a ferromagnetic body functioning as a 10 magnetic pole, at least two current carrying means and at least one shielding current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the 15 current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources first point and further assuming a first straight line 20 contained on a first plane defined by the first axis, second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying 25 means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means corresponding to the respective

projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction.

A fifth aspect of the magnet device according to the present invention in which two sets of static magnetic field generation sources, each constituted by current carrying means disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with three current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at 20 substantially the equal distance from the two sets of the static magnetic field generation sources first point and further assuming a first straight line contained on a first plane defined by the first axis, second axis and the first point and passing the through the first point, the current carrying means 25 are disposed in such a manner that, when geometrical centers of cross sections of the current carrying

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means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means corresponding to the respective projections of each of the static magnetic 5 generation sources aligns alternatively in positive and negative direction.

A sixth aspect of the magnet device according to the present invention in which two sets of static generation field sources, each magnetic 10 constituted by current carrying means and shielding carrying for suppressing leakage current means field external region disposed magnetic to an substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite 15 region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with three current carrying means and at shielding current carrying means, least one characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses orthogonally and locates first axis the substantially the equal distance from the two sets of the static magnetic field generation sources

first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means corresponding to the respective projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction.

Now, magnetic field in a magnet used in an MRI device will be explained thereinbelow.

When assuming that the center axis of the magnet device is z axis, r and  $\theta$  represent a coordinate position in a polar coordinate assuming the center of the magnet device as origin and  $Pn(\cos \theta)$  is Legendre's function of nth degree, magnetic field Bz in z direction near the center portion of the magnet device can generally be developed and expressed in the following equation (1);

$$Bz = \sum_{n=0}^{\infty} d_n r^n p_n (\cos \theta) \qquad \cdots (1)$$

wherein  $d_0$  is a uniform magnetic field and  $d_1$ ,  $d_2$ ,  $d_3$ ,  $d_4$ ,  $d_5$ ,  $d_6 \cdots$  are irregular magnetic field intensities

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which deteriorate uniformity of the magnetic field. When the magnet is arranged symmetric with respect to the center plane thereof,  $d_1$ ,  $d_3$ ,  $d_5 \cdots$  among the above irregular magnetic field components become zero because of the symmetry nature. Accordingly, only the irregular magnetic field components  $d_2$ ,  $d_4$ ,  $d_6 \cdots$  are the take into account as irregular required to magnetic fields which deteriorate uniformity of the magnetic field.

An MRI use magnet is required to form a uniform magnetic field having a few ppm order variation in an image taking region near the magnet center portion. A uniform magnetic field generation is achieved successively eliminating the irregular magnetic field 15 components  $d_2$ ,  $d_4$ ,  $d_6 \cdots$  from lower degree terms among developed terms according to equation (1) expressing a magnetic field in z direction near the center portion it will Form equation (1)of the magnet. if the irregular magnetic field understood that components are eliminated up to high degree terms, a space of uniform magnetic field will be expanded.

A magnet device for an MRI device used such as in hospitals is required to generate a uniform magnetic field within ±5ppm variation rate in a spherical region having a diameter of 40cm-50cm.

In order to fulfill the above requirement, proper magnet designs are usually employed so that

irregular magnetic field components from the second degree to 8th degree or 10th degree in that  $d_2$ ,  $d_4$ ,  $d_6$ ,  $d_8$  and  $d_{10}$  become zero.

As has been explained above, in order to generate a uniform static magnetic field, at first it is necessary to make zero the second degree irregular magnetic field component  $d_2$ .

For the sake of simplicity, a magnetic field formed by an annular ring line current is discussed.

10 Among developed terms expressed by the equation (1) of the magnetic field produced by the annular ring line current as shown in Fig. 13, plots of d<sub>2</sub> depending on β=a/b are shown in Fig. 14. Wherein, a represents a radius of the annular ring line current, b represents a distance of the annular ring line current from the origin in z axis direction and i represents a current value, and in the plots it is assumed that b=1 and i=1. As will be apparent from Fig. 14, the developed term coefficient d<sub>2</sub> becomes zero when β=2, in other words, the second degree irregular magnetic field component becomes zero with the arrangement which is already known as a Helmholtz coil.

In an MRI device use magnet, it is necessary to eliminate at first the secondary degree irregular 25 magnetic field component as has been explained above, however, as will be understood from Fig. 14, if coils

through which currents in the same direction flow are only used, it is impossible to reduce the coil diameter than that of the Helmholz coil arrangement.

ring currents Accordingly, two annular having  $\beta$  smaller than 2 as shown in Fig. 15 Wherein, it is assumed that a radius and discussed. current value of an annular ring current 175 respectively  $a_1$  and i=1, and a radius and current value of an annular ring current 176 are respectively 10  $a_2$  and i=-0.4. Values of  $d_2$  produced respectively by the two coils depending on  $\beta$  are plotted in Fig. 16. Curves 177 and 178 respectively correspond to the 175 and 176. As will annular ring currents apparent from Fig. 16, if the values  $\beta_1$  and  $\beta_2$  are 15 properly selected, it is possible to make the absolute values of respective  $d_2$  terms produced by the annular ring currents 175 and 176 equal, but the signs thereof be opposite each other, thereby, the irregular magnetic field components  $d_2$  produced by the two annular ring currents 175 and 176 can be rendered 20 Namely, through an arrangement of a plurality of coils each having different polarity in alternative radial direction the secondary degree manner in irregular magnetic field component can be eliminated 25 with coils having a smaller outer diameter than that of a Helmholz coil.

exemplary arrangement in which Now, an secondary and quadratic degree irregular magnetic field components are eliminated will be explained. Fig. 21 shows an optimum designed coil arrangement 5 which is determined through computer programs so as to minimized the sum of absolute values of magnetomotive force according to the present invention. As to eliminate 21, order in Fig. illustrated in field components up to magnetic irregular 10 quadratic degree and to reduce the outer diameter of the coils than the arrangement of a Helmholz coil, total of six pieces of coils is necessary, in that three for one of two static magnetic field generation sources and other three for the other static magnetic 15 field generation source. Coils of which current flow direction are positive and negative are alternatively arranged in the radial direction. The absolute values of magnetomotive force are increased according to the radial diameter size thereof.

How the secondary and quadratic degree irregular magnetic field components are eliminated in this coil arrangement will be explained with reference to Figs. 22 and 23.

Fig. 22 shows secondary degree irregular magnetic 25 field components produced by the respective coils shown in Fig. 21, and Fig. 23 shows quadratic degree irregular magnetic field components produced by the

respective coils as shown in Fig. 21. Curves 211, 212 and 213 are sensitivity curves relating to secondary irregular magnetic field degree components corresponding to magnetomotive forces produced coils #1, #2 and #3 in Fig. 21 with respect to  $\beta$ . Curves 214, 215 and 216 are sensitivity curves of the quadratic degree irregular magnetic field components corresponding to the magnetomotive forces of the coils #1, #2 and #3 as shown in Fig. 21 with respect to  $\beta$ . The values  $\beta$ of geometric centers of the

10 sections of the coils #1, #2 and #3 are respectively 0.30, 0.80 and 1.46. Accordingly, the secondary degree irregular magnetic field component produced by, for example, coil #3 assumes the value indicated by 15 the numeral 203. Accordingly, with the arrangement of Fig. 21 the coils #1, #2 respectively produce the secondary degree irregular magnetic field components as indicated by numerals 201, 202 and 203 in Fig. 22, and the positions and 20 magnetomotive forces of the respective coils are set so that the sum of these secondary degree irregular magnetic field components is rendered zero. the coils #1, #2 and #3 respectively produce the quadratic degree irregular magnetic field components as indicated by numerals 204, 205 and 206 in Fig. 23,

and the positions and magnetomotive forces of the

respective coils are set so that the sum of these

quadratic degree irregular magnetic field components is rendered zero.

can be qualitatively relationships These explained as follows. As has been explained above, at first it is necessary to eliminate the secondary degree irregular magnetic field components, for this reason, the positions of coils #2 and #3 are mostly Although the coil determined on this base. produces the quadratic degree irregular magnetic field component as indicated by the numeral 206 to be 10 eliminated, however, as seen from the sensitivity curves in Figs. 22 and 23, it will be understood that solution which renders both the secondary and quadratic degree irregular magnetic field components zero can not exist, only when the positions and the 15 magnetomotive forces of the coils #2 and #3 Accordingly, the coil #1 is newly added of varied. radius is t.he smallest and of which magnetomotive force is directed positive to produce irregular magnetic quadratic degree the component indicated by the numeral 204, thereby, the total sum of quadratic degree irregular magnetic field Further, in order to components is reduced zero. minimize the sum of absolute values of magnetomotive forces, the positions of the respective coils are 25 the positions determined in such a manner that corresponding near to the peaks of the respective

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sensitivity curves are avoided and the positions showing as much as small sensitivity are selected. Actually, since the coil #1 produces the secondary degree irregular magnetic field component as indicated 5 by the numeral 201, it is necessary to adjust to render the secondary degree irregular magnetic field components zero as a whole as well as the quadratic degree irregular magnetic field components accordingly an optimum arrangement of the coils is 10 correctly determined through computer programs incorporating the sensitivity curves. In order to eliminate the secondary and quadratic degree irregular magnetic field components with group of coils each having a smaller radius than that of a Helmholz coil, 15 it is necessary to arrange coils with positive and negative current flow directions alternatively as has been explained above, this is because the sensitivity irregular magnetic field components curves of respective degrees show the shapes as illustrated in Fiq. 19. The respective sensitivity curves inherently determined based on physically and electro-magnetic phenomenon. The present invention is brought about on the analysis of the sensitivity the result of the present curves, accordingly, invention which is obtained by making use of the analysis is non-ambiguously determined.

Although in the present embodiment a specific

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explanation on elimination of the irregular magnetic field components of higher degree equal to and more than 6 degree is omitted, the same principle can be through the alternate applied thereto, in that arrangement of coils having different polarity in the radial direction thereof, a magnet of which irregular magnetic field components are eliminated up to high extremely uniform degrees and which generates an magnetic field can be constituted with a magnet having a smaller outer diameter than that of a Helmholz coil. Further, the present structure provides a minimum eliminates the irregular number of coils which magnetic field components up to necessary degree, absolute values sum of the accordingly, the magnetomotive forces of the respective coils shows minimum among any conceivable coil arrangement.

above coil arrangement can be determined The of the computer making use programs through sensitivity curves of the irregular magnetic field intensities of respective degrees as shown in Fig. 19. 20 Since it is difficult to explain the function thereof, the nature of the solution is qualitatively explained. Fig. 20 shows a general space distribution of sixth degree irregular magnetic field intensity. 25 drawing, the origin represents the center of the magnet, z axis corresponds to the center axis of the magnet,  $\rho$  axis represents an axis in radial direction

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which passes through the center of the magnet and is directed to an arbitrary direction, and the abscissa sixth degree irregular magnetic field represents As will be understood from the equation intensity. (1) referred to previously, the intensity at and the intensity increases is zero proportion to 6th power of the distance according to the distance increase from the origin. depending on the nature of  $Pn(\cos \theta)$  the intensity is expressed by a space distribution having positive and negative values with respect to azimuth angle  $\theta$ . Accordingly, for example, with regard to the space distribution of 6th degree irregular magnetic field component through alternative arrangement of coils having positive and negative polarity, the 6th degree 15 irregular magnetic field component can be effectively The alternative arrangement of coils canceled out. and negative polarity can positive having generalized in such a manner that when geometric centers of cross sections of respective coils are 20 projected on a straight line passing through the origin, current polarity of the coils corresponding to the projected centers is aliqued alternatively in positive and negative on the straight line as will be defined in claims. 25

Now, advantages of the present invention will be specifically explained by making use of numerical

center portion.

calculation result. Fig. 17 shows a calculation result based on the principle of the present invention and at the same time illustrates a coil arrangement and contours representing magnetic field uniformity.

5 The respective contours of magnetic field uniformity indicate ±1, ±5 and ±10ppm from the inside. Wherein, the current density in the coils is 100A/mm², the interval between the upper and lower coils is 1.0m and the outer diameter of the coils is limited to 1.7m.

10 Further, the intensity of the center magnetic field is 0.4T and the second through 6th degree irregular magnetic field components are rendered zero near the

As will be apparent from Fig. 17, when 15 geometric centers of the respective coil cross sections on  $z-\rho$  plane in the first quadrant projected on the  $\rho$  axis, the current flow directions at the projected centers corresponding to respective coils are aligned alternatively in positive 20 and negative. With the arrangement method according to the present invention the sum of absolute values of force by the respective magnetomotive coils minimized, namely, the present method is understood the most reasonable one.

25 Fig. 18 shows one of calculation results not based on the principle of the present invention.

The current density in the coils, the intensity

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of the center magnetic field, and the degrees of canceled out irregular magnetic field components are substantially the same as these of Fig. 17. calculation example in Fig. 18, when the geometrical 5 centers of the respective coil cross sections on  $z-\rho$ plane are projected on any straight lines on the  $z-\rho$ plane passing the origin, their current directions at the projected centers corresponding to the respective coils are never aligned alternatively in positive and negative, namely, Fig. 18 arrangement never follows the principle of the present invention. When comparing the calculation example of Fig. 18 with Fig. 17, their space calculation example of distributions of generated magnetic field are substantially the same, however, in Fiq. 18 15 calculation example requires 1.4 times of the sum of absolute values of magnetomotive force produced by the coils for achieving the same space magnetic field distribution and further requires two more coils in Namely, the most advantageous effect of the total. present invention is to provide a coil arrangement which shows the minimum sum of absolute value of magnetomotive force among possible coil arrangements which produce a magnetic field distribution having a 25 predetermined space distribution. In the arrangement as shown in Fig. 18 which does not follow the principle of the present invention, since the sum

of absolute values of magnetomotive force of the coils larger when compared with the coil 1.4 times arrangement as shown in Fig. 17 which follows the principle of the present invention and the number of 5 coils also increases by 2, a variety of demerits are caused such as an increase of electro-magnetic force between coils, complexing of support structure and weight increase thereby and weight increase of cooling means, and as a result, production cost of the magnet 10 extremely increases, therefore, it is understood that the conventional design method as exemplified in Fig. inefficient one. Further, in the 18 is very calculation result as shown in Fig. 17 which is based principle of the present invention, the on absolute value of magnetomotive force of a coil having the largest average radius is larger than the absolute values of magnetomotive force of other coils and it is further understood that when the respective coils in quadrant is projected on  $\rho$  axis, the first the of the magnetomotive force absolute values of 20 aligned according the coils are respective These setting methods of the magnitudes thereof. conditions also are magnetomotive forces minimizes the sum of absolute values of magnetomotive 25 force of the entire coils.

Further, a magnet device for an open type MRI device as disclosed in U.S. Patent No.5,410,287 is directed to a horizontal magnetic field type, however, the coil arrangement therein is somewhat similar to that explained in connection with Fig. 18.

Further, for a whole-body MRI it is necessary to a uniform static magnetic field variation within ±5 ppm in a spherical region having a For this requirement it is diameter of 40cm~50cm. necessary to make zero at least up to 8th degree irregular magnetic field components, and for purpose of design freedom at least four coils are 10 necessary for each magnet assembly. In a coil design which eliminates irregular magnetic field components up to 6th degree, 8th degree irregular magnetic field dominantly controls the magnetic component 15 uniformity, therefore, it is necessary to reduce the intensity of the 8th irregular magnetic field as much possible, and for this necessary it is preferable to magnetomotive force produced by limit the Although not illustrated respective coils. 20 calculation examples here, similar calculation as in Fig. 17 and Fig. 18 examples can be performed for the case of three coils, and it is confirmed that if the three coils are arranged in the radial direction so directions therein flow that the current alternatively in positive and negative, the sum of 25 absolute values of the coil magnetomotive force is minimized.

Because of size limitation of such as a cryostat and a low temperature vessel, necessary number of coils can not sometimes be disposed in the radial direction, in such instance, it is sufficient if a coil is disposed along the inner wall of the low temperature vessel. The present invention discloses such generalized coil arrangement methods, and the specific examples thereof will be explained as embodiments hereinbelow.

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## BRIEF DESCRIPTION OF THE DRAWINGS

- Fig. 1 is a perspective view of an open type MRI device using a super conducting magnet according to the present invention;
- Fig. 2 is a cross sectional view of a super conducting magnet representing an embodiment according to the present invention;
- Fig. 3 is a cross sectional view of a super conducting magnet representing another embodiment 20 according to the present invention;
  - Fig. 4 is a cross sectional view of a super conducting magnet representing still another embodiment according to the present invention;
- Fig. 5 is a cross sectional view of a super 25 conducting magnet representing a further embodiment according to the present invention;
  - Fig. 6 is a cross sectional view of a super

conducting magnet representing a still further embodiment according to the present invention;

Fig. 7 is a cross sectional view of a super conducting magnet representing a still further 5 embodiment according to the present invention;

Fig. 8 is a cross sectional view of a super conducting magnet representing a still further embodiment according to the present invention;

Fig. 9 is a cross sectional view of a super 10 conducting magnet representing a still further embodiment according to the present invention;

Fig. 10 is a cross sectional view of a super conducting magnet representing a still further embodiment according to the present invention;

Fig. 11 is a cross sectional view of a super conducting magnet representing a still further embodiment according to the present invention;

Fig. 12 is a cross sectional view of a super conducting magnet representing a still further 20 embodiment according to the present invention;

Fig. 13 is a view for explaining an annular ring current;

Fig. 14 is a diagram showing a sensitivity curve of secondary degree irregular magnetic field intensity produced by the annular ring current as shown in Fig. 13;

Fig. 15 is a view for explaining two annular ring

currents;

Fig. 16 is a diagram showing sensitivity curves of second degree irregular magnetic field intensity produced by the two annular ring currents as shown in 5 Fig. 15;

Fig. 17 is a diagram showing a numerical calculation example of a coil arrangement according to the present invention and contours of the magnetic field uniformity produced thereby;

10 Fig. 18 is a diagram showing a numerical calculation example of a coil arrangement according to the present invention and contours of the magnetic field uniformity produced thereby;

Fig. 19 is a diagram showing sensitivity curves of irregular magnetic field intensities from second degree to 6th degree produced by the annular ring current as shown in Fig. 13;

Fig. 20 is three dimensional plots showing a space distribution of 6th degree irregular magnetic 20 field component;

Fig. 21 shows an optimum designed coil arrangement through computer programs so that the sum of absolute values of magnetomotive force is minimized according to the principle of the present invention;

Fig. 22 shows second degree irregular magnetic field components produced by the respective coils as shown in Fig. 21; and

Fig. 23 shows 4th degree irregular magnetic field components produced by the respective coils as shown in Fig. 21.

BEST MODES FOR CARRYING OUT THE PRESENT INVENTION
Hereinbelow, embodiments of the present invention
will be explained specifically with reference to Fig.
1 through Fig. 12.

Fig. 1 is a perspective view of an open type super conducting MRI device using a super conducting magnet representing an embodiment according to the present invention. Fig. 2 is a cross sectional view on z-x plane of the super conducting magnet 1 among many constituting elements of the open type MRI device in Fig. 1.

The MRI device as shown in Fig. 1 produces a uniform magnetic field in z axis direction in an open region 2 by upper and lower super conduction magnet assemblies 6 and 7, and permits MRI image taking at the center portion of the open region 2. A patient 4 20 is carried by a bed and movable table 3 so that an image taking portion of the patient 4 positions at the center portion of the open region 2. The upper and lower super conducting magnetic assemblies 6 and 7 are column shaped external by coupled 25 magnetically ferromagnetic bodies 10 and are further designed so as leakage magnetic field. With thus suppress to

structured MRI, claustrophobia to which the patient 4 tends to be subjected during image taking is extremely reduced and the patient 4 can even be given an open space feeling, thereby, a psychological pressure of the patient 4 with respect to the image taking is Further, an access of a medical greatly reduced. doctor or an inspection engineer 5 to the patient 4 be facilitated taking can during the image In particular, an access of the significantly. medical doctor or the inspection engineer 5 to an 10 object portion of the patient 4 during the image taking is permitted, therefore, an Interventional Radiology (IVR) is enabled which broadens possibility of medical treatment.

15 Further, as an advantage of the MRI device having the structure as shown in Fig. 1, since the direction of static magnetic field is orthogonal with respect to the longitudinal direction of a human body, a solenoid coil can be used for a probe for receiving NMR 20 signals. The sensitivity of such solenoid type probe is theoretically 1.4 times higher than that of a saddle shaped or bird cage shaped probe used for the horizontal magnetic field type MRI device.

Accordingly, when assuming that the center 25 magnetic field intensity is equal each other, the vertical magnetic field type MRI having the structure as shown in Fig. 1 can take a further accurate

tomographic images with a further higher speed in comparison with the conventional horizontal magnetic field type MRI device.

As has been mentioned above, the MRI device structured according to the concept as shown in Fig. 1 has a variety of advantages, however, a key for achieving a highly open space feeling from structural point of view is how to reduce the diameter of the upper and lower magnetic assemblies 6 and 7. The present invention exactly relates to the key and provides a magnet assembly structure of which outer diameter is small and of which production cost is inexpensive, and moreover which generates a desired uniform magnetic field.

Now, the structure of the magnet assemblies 6 and 15 7 will be explained with reference to Fig. 2. The magnet assemblies 6 and 7 are upper and lower surrounded at the outer circumferences thereof by respective ferromagnetic bodies so as to suppress leakage magnetic field. specifically, More 20 shaped external ferromagnetic bodies 8 and 8' cylindrical external ferromagnetic bodies 9 and surround around upper and lower vacuum vessels 11 and 11', and the upper and lower ferromagnetic bodies 8, 8' and 9, 9' are magnetically coupled by the column 25 shaped external ferromagnetic bodies 10. As the external ferromagnetic bodies used in the present

embodiment, any material will do, if such shows ferromagnetic property so that a variety of material can be used, however, in view of magnetic properties, ion is generally strength mechanical cost and 5 preferable. Further, when a weight lightening of the ferromagnetic bodies is required, a material having a Through permeability can be used. high surrounding of the circumferences with the external ferromagnetic bodies magnetic passages are formed for magnetic fluxes possibly leaking outside from the 10 device to thereby suppress the leakage magnetic field from expanding far.

Main super conducting coils 13, 13', 14, 14', 15, 15' and 16, 16' are disposed substantially symmetric in upper and lower positions while sandwiching a 15 uniform magnetic field region at the center of the magnet and substantially concentrically with respect to z axis, and produces a uniform magnetic field in vertical direction, namely in z axis direction. The 20 upper and lower super conducting coils are disposed inside respective cooling containers 12 and 12', and the upper and lower cooling containers 12 and 12' are accommodated in respective vacuum vessels 11 and 11'. Further, for the sake of simplicity although the 2 is omitted, there is Fiq. illustration in 25 structure for supporting the super conducting coils and further there is provided a heat shielding member

between the vacuum vessels and the cooling containers for preventing penetration of radiation heat. helium is stored inside the cooling vessels and cools the super conducting coils to a super low temperature of 4.2°K.

The upper and lower vacuum vessels are held by coupling tubes 17 disposed therebetween while keeping These coupling tubes 17 a predetermined distance. work to support mechanically the upper and lower 10 vacuum vessels 11 and 11', however, can include a function of thermally connecting the upper and lower If such function is added, it cooling containers. becomes unnecessary to provide each one cryostat for lower cooling containers, thereby, the upper and system can be operated with a single cryostat. Further, the number of the coupling tubes 17 and the column shaped ferromagnetic bodies 10 needs not to be limited to two as illustrated, but can be increased three, four and more. Further, in order to obtain a 20 further open space feeling a single support column forming an overhang structure can be used.

In the present embodiment, the respective four main super conducting coils 13, 13', 14, 14', 15, 15' and 16, 16' inside the respective upper and lower magnet assemblies are arranged so as to align their polarities alternatively in positive and negative. More precisely, when assuming a certain straight line

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18 passing through the center of the magnet assemblies on any plane containing z axis representing the center sake for the magnet (herein, of the explanation simplicity z-x plane is assumed) and when the geometric center of the cross sections of the conducting coils in the super respective z-x plane are projected quadrant on the straight line 18, the polarities of current flow of the projections on the straight line 18 corresponding respective coils alternatively align In other words, in the coil 16 positive and negative. a current is flown to the direction causing the main magnetic field and of which direction is assumed as the positive direction, a current in the negative direction is flown in the coils 13 and 15, and a current in positive direction is flown in the coil 14.

Further, as seen from the drawing, the magnitude of absolute values of magnetomotive force of the respective coils 16, 15, 14 and 13 is larger in this appearing order and it is understood that when the respective coils in the first quadrant on the plane are projected on the straight line 18, magnetomotive force values of absolute respective coils align in their order of magnitude. Further, the absolute value of magnetomotive force of 25 the coil 16 having the maximum average radius is the These magnetomotive force setting method is largest.

also one of the conditions which minimizes the sum of absolute values of magnetomotive force of the entire coils.

The positions and magnetomotive forces of the 5 respective coils are designed based on calculations so as to form a uniform magnetic field distribution. Although arrangement of coils which produces a uniform however, the field is infinite, magnetic method as has been explained in the arrangement 10 Summary of the Invention gives the minimum sum of absolute values of magnetomotive force, thereby, the magnet can be produced with minimum cost. Further, since the sum of absolute values of magnetomotive small, the cross sectional areas of the force is 15 respective coils are reduced, thereby, the diameters of the magnet assemblies can also be reduced. further, the present embodiment is designed to render the irregular magnetic field components from second degree to 8th degree zero, and for this purpose four 20 coils are disposed in respective magnet assemblies. As a result, a uniform magnetic field of 45cm dsv (diameter of spherical volume) with ±4 ppm variation obtained at the center of the magnet which sufficiently fulfills the specification for a wholebody MRI. 25

Hereinbelow, other embodiments according to the present invention will be explained with reference to

the drawings.

Fig. 3 is a cross sectional view of a super conducting magnet for an open type MRI representing another embodiment according to the present invention. 5 The constitutional structure of the present embodiment is substantially the same as the super conducting magnet as shown in Figs. 1 and 2 except for a provision of super conducting shielding coils 29 and of the external wéight the reducing 29' for bodies suppressing leakage magnetic ferromagnetic general naming of leakage According to field. magnetic field shielding methods, the method of Fig. 2 embodiment is called as a passive shielding method and the method of Fig. 3 embodiment is called as a hybrid shielding method. When the geometric centers of the 15 cross sections of main super conducting coils 25, 25', 26, 26', 27, 27' and 28, 28' except for the super conducting shielding coils 29 and 29' in Fig. 3 on the z-x plane in the first quadrant are projected on a 20 straight line 30 (an imaginary line), the coils are arranged in such a manner that the current flow the corresponding coils to the of direction in positive alternatively and aligns projections negative on the straight line 30.

Fig. 4 is a cross sectional view of a super conducting magnet for an open type MRI device representing still another embodiment according to the

present invention. The present embodiment shows an active shielding type super conducting magnet. The present embodiment suppresses leakage magnetic field shielding coils and by the shielding bodies such ferromagnetic as iron. therefore, the weight thereof is minimized. When the geometric centers of the cross sections of main super conducting coils 34, 34', 35, 35', 36, 36' and 37, 37' except for the super conducting shielding coils 39 and 10 39' in Fig. 4 on the z-x plane in the first quadrant are projected on a straight line 40, the coils are arranged in such a manner that the current flow corresponding direction coils the of the to aligns alternatively in positive projections and negative on the straight line 40. 15

In the above embodiment, the magnet assemblies constituted basically to produce a uniform magnetic field by air-core coils and to suppress leakage magnetic field by the external ferromagnetic shielding coils. Hereinbelow, 20 bodies or the embodiments according to the present invention which makes use of ferromagnetic positively functioning as magnetic poles for producing uniform magnetic field are disclosed. Figs. 5 through sectional views of super conducting are cross 25 12 magnets for an open type MRI representing further embodiments according to the present invention.

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The magnet as shown in Fig. 5 is designed in such a manner that magnetic pole shaped ferromagnetic bodies 44 and 44' disposed inside disk shaped external ferromagnetic bodies 41 and 41' function to enhance the center magnetic field intensity and to reduce the share to be borne by the super conducting coils for the center magnetic field intensity as well as to reduce the sum of absolute values of magnetomotive force of the super conducting coils. Since the uniformity of magnetic field is primarily achieved by the arrangement of the super conducting coils and the division manner of their magnetomotive forces, the present arrangement is based on the principle of the present invention. Namely, where the geometric 15 centers of the cross sections of main super conducting coils 48, 48', 49, 49', 50, 50' and 51, 51' in Fig. 5 on the z-x plane in the first quadrant are projected on a straight line 52, the coils are arranged in such a manner that the current flow direction of corresponding coils to the projections alternatively in positive and negative on the straight line 52.

In the magnet as shown in Fig. 6, the magnetic poles are further enlarged in comparison with the magnet as shown in Fig. 5 and the burden with regard to magnetomotive forces of super conducting coils is present embodiment further reduced. The is

constituted to optimize the shape of the magnetic poles and to produce a certain level of uniform poles. the magnetic only with magnetic field Accordingly, a small number of super conducting coils will do and in the present embodiment each two super conducting coils in respective upper and lower magnet assemblies can produce sufficient uniform magnetic As has been explained in the Summary of the field. Invention, the current flow direction of the two super conducting coils 60, 60' and 61, 61' are opposite each other, thereby, the second degree irregular magnetic field components are eliminated with the small magnet assemblies. Namely, a current is flown in the outside super conducting coils in the direction producing the main magnetic field. On the other hand, a current in the opposite direction is flown in the inside super conducting coils.

In the magnet as shown in Fig. 7, a rough uniform magnetic field is produced by the magnetic poles having an optimized configuration and three super 20 conducting coils are disposed in the respective magnet assemblies so as to further enhance the uniformity of The main super conducting coils the magnetic field. 70, 70', 71, 71' and 72, 72' are arranged so as to produce a uniform magnetic field with a limited radius and with a minimum magnetomotive force in such a the direction of flow that the current manner

corresponding coils to the projections aligns alternatively in positive and negative on the straight line 73 as shown in Fig. 7 according to the principle of the present invention.

- A magnet as shown in Fig. 8 is substantially the same as the magnet as shown in Fig. 7 except for the provision of super conducting shielding coils 84 and of 84' for reducing the weight the external ferromagnetic bodies for suppressing leakage magnetic field. In the present embodiment, the main super conducting coils 81, 81', 82, 82' and 83, 83' except for the shielding coils 84 and 84' are arranged so as to produce a uniform magnetic field with a limited radius and with a minimum magnetomotive force in such a manner that the current flow direction 15 of corresponding coils to the projections aligns alternatively in positive and negative on the straight line 85 as shown in Fig. 8 according to the principle of the present invention.
- Figs. 9 and 10 are other embodiments of super conducting magnets for an open type MRI which produce a uniform magnetic field through combinations of magnetic poles and super conducting coils. The both magnets are principally constituted based on the following concept that the magnetic poles functions to strengthen the center magnetic field intensity so as to save magnetomotive forces of the coils and the

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uniformity of the magnetic field is achieved by the arrangement of the coils. Although the configuration of magnetic pole shaped ferromagnetic bodies 89, 89' 101, 101' is optimized, since the bodies are located away from the center portion of the magnet serving as the image taking region, it is impossible uniform magnetic field only with produce the magnetic pole configuration. modification of the Therefore, in Figs. 9 and 10 embodiments, with four and three super conducting coils for each assembly a uniform magnetic field is produced. Further, in Fig. 10 embodiment, the outer circumferential portions of vacuum vessels 102 and low temperature containers 103 are expanded so as to receive the end portion coils 107 having a larger magnetomotive forces. Further, with such configuration, the magnetic pole shaped ferromagnetic bodies 101 and 101' can be located near to the image taking region, thereby the share borne by magnetic poles for strengthening the the magnetic field intensity can be increased, thus the be the to borne by super magnetomotive force conducting coils is saved. The main super conducting coils in both embodiments are arranged so produce a uniform magnetic field with a limited radius and with a minimum magnetomotive force in such a current direction of the the flow manner that the projections aligns corresponding coils to

alternatively in positive and negative on the straight line 97 or x axis 108 as shown in Fig. 9 or 10 according to the principle of the present invention.

Figs. 11 and 12 show further embodiments in which ferromagnetic body elements are disposed inside the low temperature containers primarily for reducing the magnetomotive forces to be induced by the coils. regard to leakage magnetic field suppressing method, Fig. 11 embodiment uses a passive shielding method and 10 Fig. 12 embodiment uses an active shielding method. Inner ferromagnetic bodies 119, 119', 120, 120' and 131, 131', 132, 132' are formed in an annular ring shape and are disposed respectively between super conducting coils. When disposing these ferromagnetic body elements in such position, the magnetomotive 15 forces to be induced by the coils can be effectively reduced. Likely, in the present embodiments, the super conducting coils constituting the main coils are arranged so as to produce a uniform magnetic field with a limited radius and with a minimum magnetomotive force in such a manner that the current flow direction of the corresponding coils to the projections aligns alternatively in positive and negative on the straight line 122 or 133 as shown in Fig. 11 or 12 according to the principle of the present invention. 25

Hitherto, the present invention has been explained with reference to the concrete embodiments.

In the above embodiments, all of the coils were super conducting coils, however, the coils according to the the limited to not invention are present For example, coils using copper conducting coils. 5 wires can be used, further, any materials which carry current can be acceptable. For the present invention a variety of embodiments can be conceived a part of which has been explained above, therefore, the present invention should never be limited to the specific embodiments disclosed. 10

As has been explained hitherto, according to the present invention, a super conducting magnet, device for an open type MRI which is provided with a broad opening and is obtainable a broad uniform magnetic 15 field production region with a high magnetic field intensity and with less leakage magnetic field and improved which further is being stable in time, higher open space feeling and further provides a permits a desirable access to a patient representing 20 an inspection object through reducing the diameter of the magnet which also permits manufacturing cost reduction.

Further, according to the present invention, an MRI device can be realized which provides a higher open feeling and permits a desirable access to an inspection object.

## INDUSTRIAL FEASIBILITY

As has been explained above, the magnet device according to the present invention is useful for a magnet device for a medical treatment use MRI device, in particular applicable for a super conducting magnet device for an open and vertical magnetic field type MRI device.

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- A magnet device in which two sets of static magnetic field generation sources, each being 1. constituted by current carrying means disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with at least four current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.
- 2. A magnet device in which two sets of static magnetic field generation sources, each being constituted by current carrying means and shielding current carrying means for suppressing leakage magnetic field to an external region disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite

region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with at least four current carrying means and at least one shielding current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.

3. A magnet device in which two sets of static magnetic field generation sources, each being constituted by current carrying means disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with a ferromagnetic body functioning as a magnetic pole and at least two current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis

orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.

4. A magnet device in which two sets of static magnetic field generation sources, each being constituted by current carrying means and shielding current carrying means for suppressing leakage magnetic field to an external region disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with a ferromagnetic body functioning as a magnetic pole, at least two current carrying means and at least one shielding current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner

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that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.

- 5. A magnet device in which two sets of static magnetic field generation sources, each being constituted by current carrying means disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with three current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.
- 6. A magnet device in which two sets of static magnetic field generation sources, each being constituted by current carrying means and shielding current carrying means for suppressing leakage

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magnetic field to an external region disposed substantially concentrically with respect to a first direction in order to generate a uniform magnetic field directing in the first direction in a finite region, are disposed facing each other while placing the uniform magnetic field region therebetween and each of the static magnetic field generation sources is provided with three current carrying means and at least one shielding current carrying means, characterized in that when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of each of the static magnetic field generation sources aligns alternatively in positive and negative direction on the first straight line.

7. A magnet device according to one of claims 1-4, characterized in that when the geometric centers of the cross sections of the current carrying means are projected on the first straight line on the first plane, the absolute values of magnetomotive force of the current carrying means in the respective static magnetic field generation sources at the corresponding projections align on the first straight line in either descending order or ascending order.

- 8. A magnet device according to claim 5-6, characterized in that when the geometric centers of the cross sections of the current carrying means are projected on the second axis on the first plane, the absolute values of magnetomotive force of the current carrying means in the respective static magnetic field generation sources at the corresponding projections align on the second axis in either descending order or ascending order.
- 9. A magnet device according to one of claims 1-8, characterized in that in each of the static magnetic field generation sources, the absolute values of magnetomotive force of the current carrying means having the largest average radius among the current carrying means is larger than the absolute values of the magnetomotive force of other currently carrying means.
- 10. A magnet device according to one of claims 1-9, characterized in that each of the static magnetic field generation sources includes at least one ferromagnetic body which helps formation of the magnetic field.
- 11. A magnet device according to claim 10, characterized in that the ferromagnetic body functions as a magnetic pole.
- 12. A magnet device according to one of claims 1-11, characterized in that the magnetic device further comprises an external ferromagnetic body which covers the outside of the two sets of static magnetic field generation sources and forms a magnetic passage to suppress leakage magnetic field.

- 13. A magnet device according to claim 12, characterized in that the external ferromagnetic body includes a disk shaped ferromagnetic body and a column shaped ferromagnetic body.
- 14. A magnet device according to one of claims 1-13, characterized in that the current carrying means is constituted by a material having a super conducting property, and the two sets of static magnetic field generation sources includes a cooling means which cools the current carrying means to a temperature at which the current carrying means shows the super conducting property and maintains the same at the temperature.
- 15. An MRI device which uses the magnet device according to one of claims 1-14.
- 16. An MRI device including the magnet device according to one of claims 1-14, which applies the magnetic field in such a manner that the main magnetic flux direction is perpendicular with respect to the face of a stand on which a measurement object is laid.
- 17. A super conducting magnetic device for an open and vertical magnetic field type MRI device including a first and a second static magnetic field generation source which are disposed in vertical direction opposing each other while sandwiching a space for receiving a person to be inspected, each of the first and second static magnetic filed generation sources includes static magnetic filed generation use coil units of equal to or more than three which are arranged concentrically around the center axis in vertical direction thereof, characterized in that, the directions of DC current flow in the static magnetic field generation use coil units of equal to or

more than three in each of the static magnetic field generation sources are determined alternative in positive and negative direction with reference to projection positions of geometric centers of cross sections of the respective coil units of equal to or more than three on a straight line passing through a crossing point, on a plane which is perpendicular to the central axis in vertical direction and contains a horizontal axis having an equal distance both from the first and second static magnetic field generation sources, of the center axis and the horizontal axis and at the side of the straight line away from the horizontal axis when viewed from the respective coil units of equal to or more than three.

18. A super conducting magnet device for an open and vertical magnetic field type MRI device including a pair of static magnetic field generation sources which are disposed in vertical direction opposing each other while sandwiching a space having a broad opening for receiving a person to be inspected, and each of the pair of static magnetic field generation sources includes a main coil unit for the static magnetic field generation having first diameter and being disposed concentrically with the center axis in vertical direction thereof, a plurality of coil units for irregular magnetic field correction each having a diameter smaller than the first diameter and being likely disposed concentrically with the center axis in vertical direction thereof and shielding coil unit for suppressing magnetic field leakage having substantially the same diameter as the first diameter and being disposed concentrically with the center axis in vertical direction thereof but being located distant position than the main coil unit for static magnetic field generation with respect to the space, characterized in that, the directions of DC current flow in the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic filed

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correction in each of the static magnetic field generation sources are determined alternative in positive and negative direction with reference to projection positions of geometric centers of cross sections of the main coil unit for static magnetic field generation and the plurality of the coil units for irregular magnetic field correction on a straight line passing through a crossing point, on a plane which is perpendicular to the center axis in vertical direction and contains a horizonal axis having an equal distance both from the first and second static magnetic field generation sources, of the center axis and the horizontal axis and at the side of the straight line away from the horizonal axis when viewed from the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic field correction, as well as the direction of DC current flow in the shielding coil unit is determined to be opposite to the direction of the DC current flow in the main coil unit for static magnetic field generation.

19. A magnetic device including a pair of static magnetic field generation sources for generating a uniform magnetic field directing in a first direction in a finite region each of the static magnetic field generation sources being provided with at least two current carrying means disposed concentrically, characterized in that, the at least two current carrying means are disposed concentrically while being spaced each other and further when assuming a crossing point of a first axis which is in parallel with the first direction and passes substantially the center of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the respective static magnetic field generation sources as a first point, the current carrying means are disposed in such a manner that when geometrical centers of cross sections of the current carrying means are projected on a first straight line on a

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first plane containing the first axis, the second axis and the first point and passing through the first point, the current carrying means at the respective corresponding projections aligns alternatively in positive and negative direction on the first straight line.

A super conducing magnetic device for an open and vertical magnetic field type MRI device including a first and a second static magnetic field generation source which are disposed opposing each other while sandwiching a space for receiving a person to be examined, each of the first and second static magnetic field generation sources includes static magnetic field generation use coil units of equal to or more than three which are arranged concentrically with the central axis passing through the center thereof, characterized in that, the static magnetic field generation use coil units of equal to or more than three in each of the static magnetic field generation sources are arranged in such a manner that within an angle range defined by a first line segment on a plane containing the center axis and extending in a direction perpendicular to the center axis from a center point on the center axis having substantially the same distance from both first and second static magnetic field generation sources and a second line segment extending from the center point toward the static magnetic field generation use coil unit located most inside and most close with respect to the space within the plane, when the geometric centers of the cross sections of the respective static magnetic field generation use coil units are projected on any straight line while locating the first line segment therebetween, the current flow directions of the static magnetic field generation use coil units at the respective corresponding projection points align alternatively in positive and negative direction on the straight line.

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A super conducting magnet device for an open and vertical magnetic field type MRI device 21. including a pair of static magnetic field generation sources which are disposed opposing each other while sandwiching a space having a broad opening for receiving a person to be examined, and each of the pair of static magnetic field generation sources includes a main coil unit for the static magnetic field generation having a first diameter and being disposed concentrically with the center axis passing the center of the static magnetic field generation sources, a plurality of coil units for irregular magnetic field correction each having diameter smaller than the first diameter and being disposed concentrically with the center axis thereof and a shielding coil unit for suppressing magnetic field leakage having substantially the same diameter as the first diameter and being disposed concentrically with the center axis thereof but being located distant position than the main coil unit for static magnetic field generation with respect to the space, characterized in that, the main coil unit for static magnetic field generation and the plurality of coil units for irregular magnetic field correction in each of the static magnetic field generation sources are arranged in such a manner that within an angle range defined by a first line segment on a plane containing the center axis and extending in a direction perpendicular to the center axis from a center point on the center axis having substantially the same distance from both first and second static magnetic field generation sources and a second line segment extending from the center point toward the coil unit for irregular magnetic field correction located most inside and most close with respect to the space within the plane, when the geometric centers of the cross sections of the main coil unit for static magnetic field generation and the plurality of unit coils for irregular magnetic field correction are projected on any straight line while locating the first line segment therebetween, the current flow directions of the mail coil unit for static magnetic field

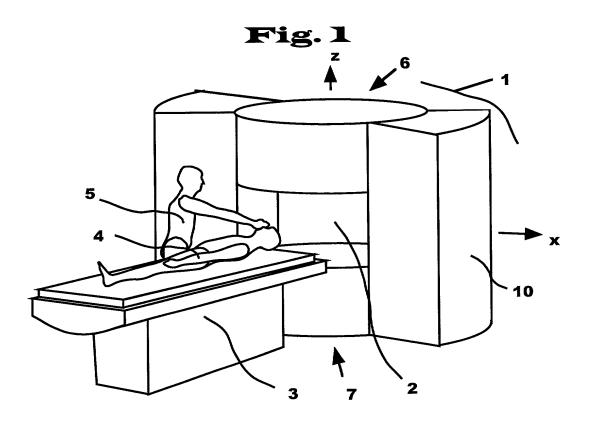
generation and the plurality of unit coils for irregular magnetic field correction at the respective corresponding projection points align alternatively in positive and negative direction on the straight line as well as the direction of DC current flow in the shielding coil unit is determined to be opposite to the direction of the DC current flow in the main coil unit for static magnetic field generation.

## ABSTRACT OF THE DISCLOSURE

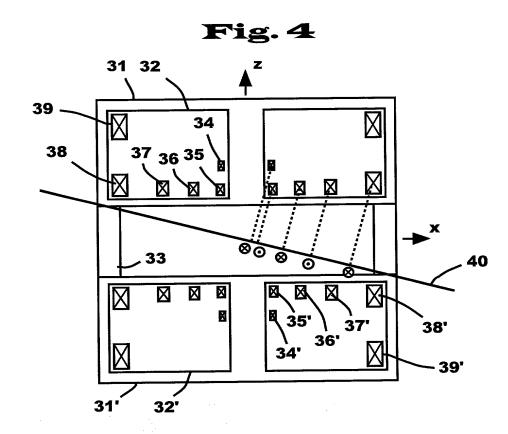
A magnet device which includes two sets of static field generation magnetic sources, each constituted by current carrying means disposed concentrically in order to generate a uniform magnetic field directing in a first direction being provided with at least four current carrying means, and in which when assuming a crossing point of a first axis 10 which is in parallel with the first direction and substantially the center passes of the current carrying means and a second axis which crosses the first axis orthogonally and locates at substantially the equal distance from the two sets of the static magnetic field generation sources as a first point and 15 further assuming a first straight line contained on a first plane defined by the first axis, the second axis and the first point and passing through the first point, the current carrying means are disposed in such 20 a manner that, when geometrical centers of cross sections of the current carrying means on the first plane are projected on the first straight line, the current carrying direction of the current carrying means at the respective corresponding projections of 25 each of the static magnetic field generation sources alternatively positive and negative aligns in direction on the first straight line, thereby, an open

space feeling and accessibility to an object to be inspected are improved in an MRI device.

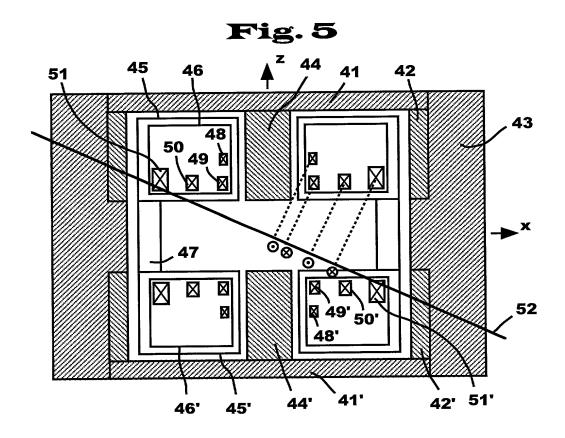
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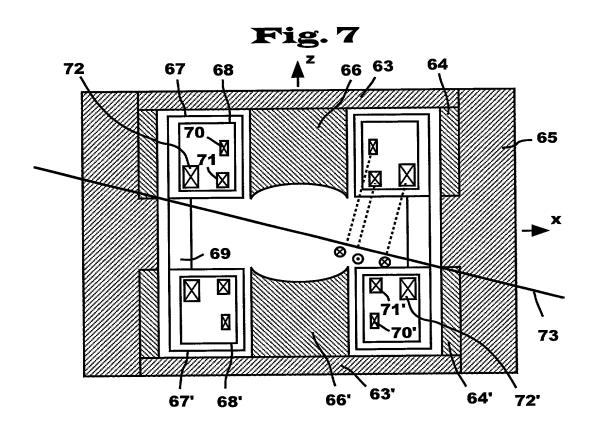


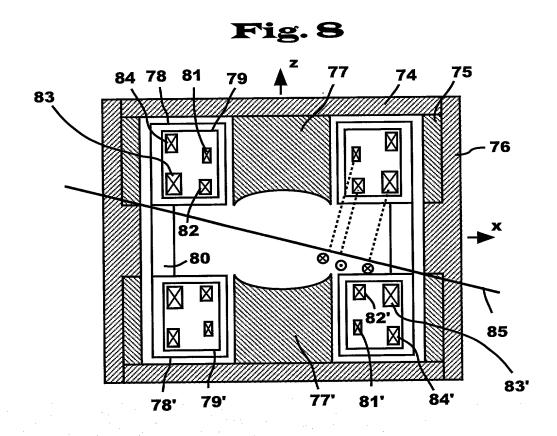
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Fig. 6

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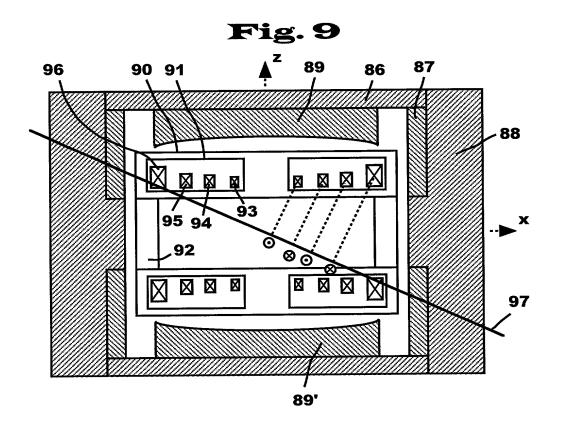
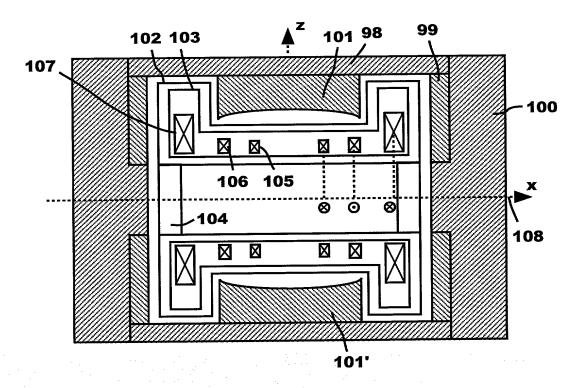
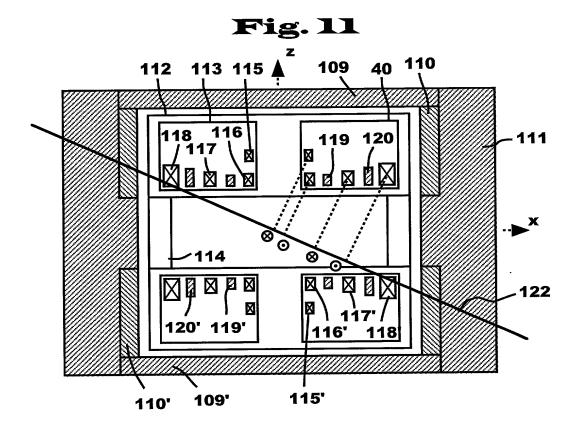
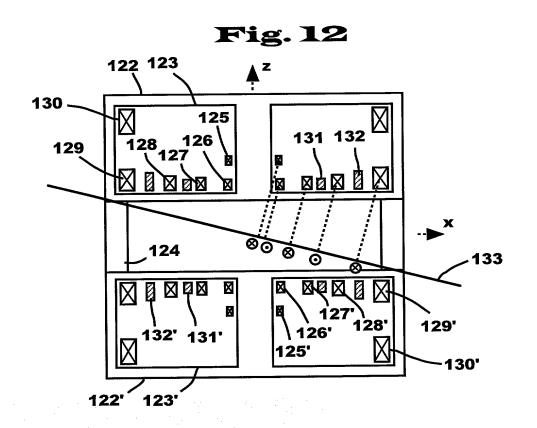


Fig. 10



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Fig. 13

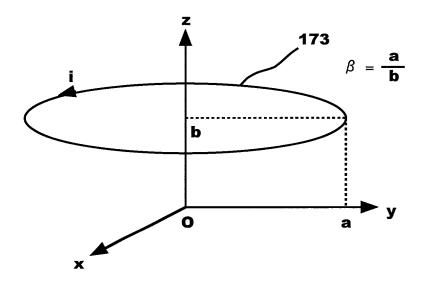
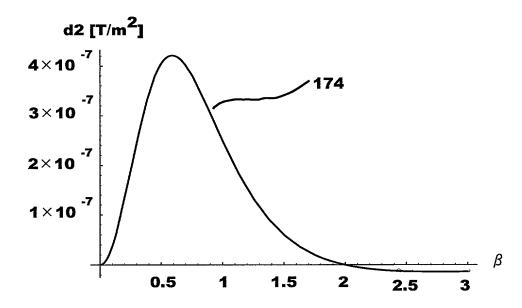


Fig. 14



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Fig. 15

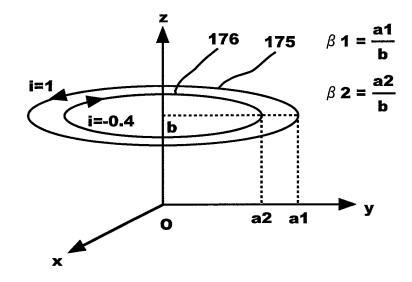
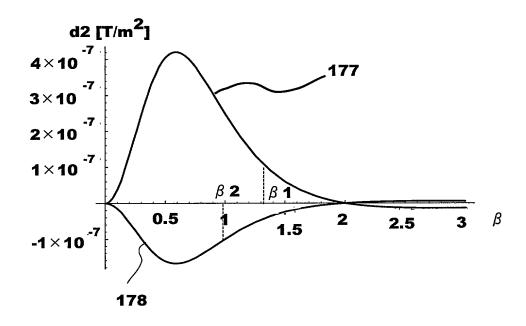
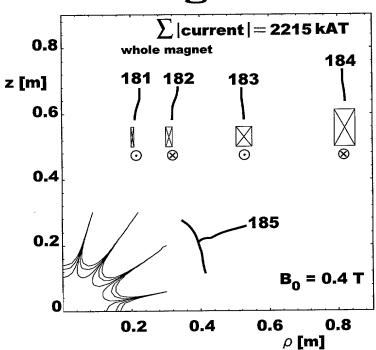


Fig. 16

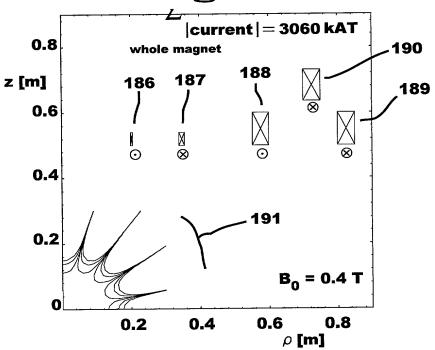


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Fig. 17







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Fig. 19

# IRREGULAR MAGNETIC FIELD INTENSITY

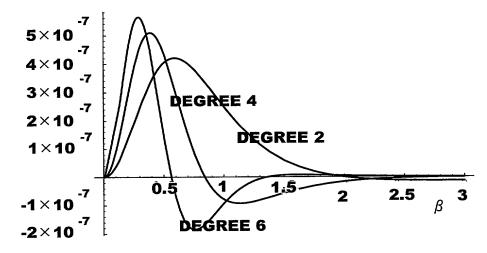
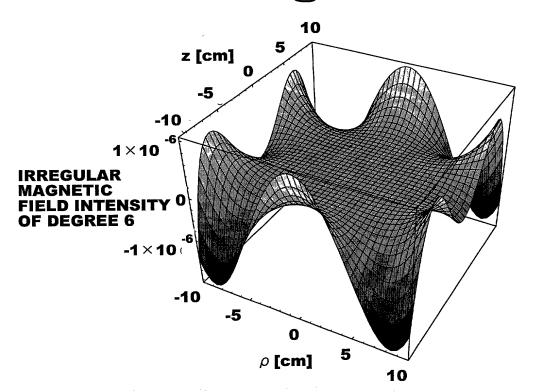


Fig. 20



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Fig. 21

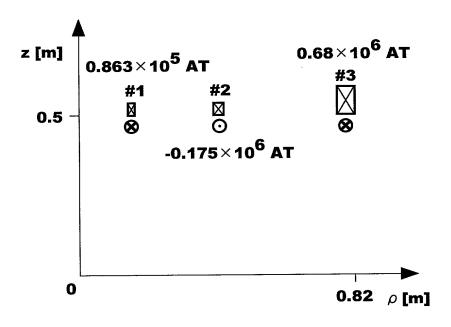
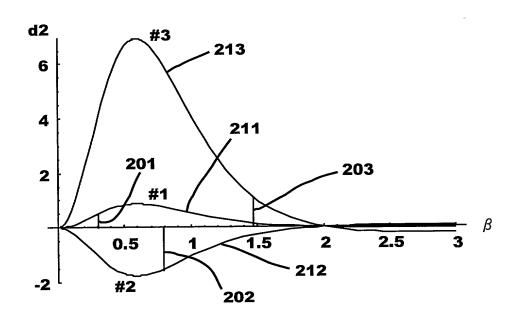
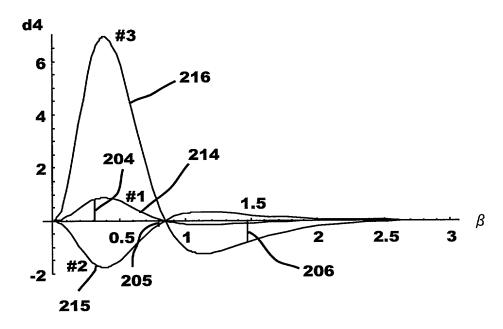


Fig. 22



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Fig. 23



### Japanese Language Declaration

(日本語宣言書)

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 PCT/JP98/05406
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(出願番号) (出願日)

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Priority Not Claimed 優先権主<del>張</del>なし

O1、12、98

(Day/Month/Year Filed)
(出類年月日)

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(出類年月日)

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(Application No.) (Filing Date) (出願音)

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### Japanese Language Declaration

### 日本語宣言書

マコル氏名が多明者として、私は以下の通り宣言します。

As a below named inventor, I hereby declare that:

私の住所、私書箱、国籍は下記の私の氏名の後に記載され た通りです

My residence, post office address and citizenship are as stated next to my name.

下記の名称の発明に関して請求範囲に記載され、特許出顧している発明内容について、私が最初かつ唯一の発明者(下記の氏名が一つの場合)もしくは最初かつ共同発明者であると(下記の名称が複数の場合)信しています。	I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claumed and for which a patent is sought on the invention entitled
MAGNET APPARATUS AND MRI APPARA	ATUS
上記発明の明細書(下記の欄でxáiがついていない場合は、 本書に茶付)は、	the specification of which is attached hereto unless the following box is checked:
□    □    □    □    □    □    □	was filed on as United States Application Number or PCT International Application Number and was amended on (if applicable).
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I acknowledge the duty to disclose information which is material to patentability as defined in Title 37, Code of Federal Regulations, Section 1.56.

Page 1 of 3

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# Japanese Language Declaration

(日本語宣言書)

委任状・ 弘は下記の発明者として、本出顧に関する一切の 子続きを米特許新標局に対して遂行する弁理士または代理人 として、下記の者を指名いたします。(弁護士、または代理 への氏名及び登録番号を明記のこと) POWER OF ATTORNEY: As a named inventor, I hereby appoint the (ollowing attorney(s) and/or agent(s) to prosecute this application and transact all business in the Patent and Trademerk Office connected therewith (Est name and registration number)

Ivan S. Kavrukov (Reg. No. 25161), Thomas F. Moran (Reg. No. 16579); Christopher C. Dunham (Reg. No. 22031); Norman H. Zivin (Reg. No. 25385), John P. White (Reg. No. 28678); Robert D. Katz (Reg. No. 30141); Peter J. Phillips (Reg. No. 29691); Richard S. Milner (Reg. No. 33970); Richard F. Jaworski (Reg. No. 33515); and Paul Teng (Reg. No. 40837)

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、名前及ひ電話番号)

(第三以降の共同発明者についても同様に記載し、署名をす

Direct Telephone Calls to: (name and telephone number)

(Supply similar information and signature for third and subsequent

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